

Factors for validation of measurement-based simulations

David Sinden¹, Srinath Rajagopal², Piero Miloro², Bajram Zeqiri²

david.sinden@mevis.fraunhofer.de

ASA 179: Acoustics Virtually Everywhere

Tuesday 8 December 2020

¹ Fraunhofer Institute for Digital Medicine MEVIS, Bremen, Germany

² National Physical Laboratory, Teddington, United Kingdom

Introduction

Acoustic Equations

Acoustic Holography

Data Quality

Post-Acoustics Computation

Heat Equations

Dose Equations

Updating Equations

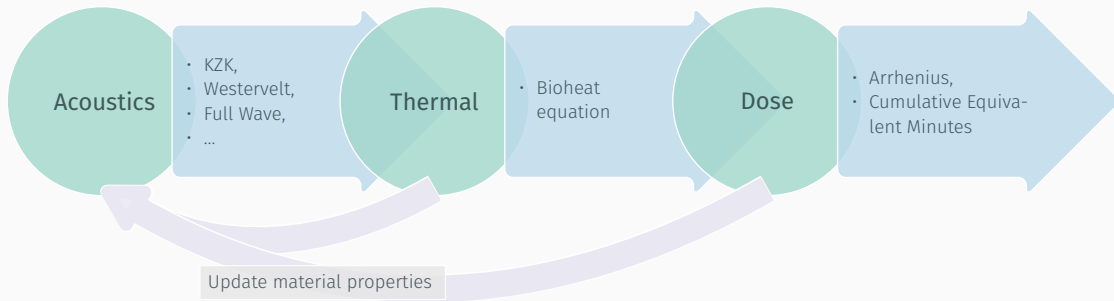
Measurements

Acoustics Measurements

Thermal & Dosimetric Measurements

Conclusions

A Simulation Process



- The acoustic equations may be an **order of magnitude** more computationally expensive than the thermal equations, which may be an order of magnitude more computationally expensive than the dose equations.

Why Simulations? Why Measurement-based Simulations?

Advantages

- Measurements enable transducer performance to be assessed
- Ability to predict pressures in regions where it is not possible to make measurements, for example due to inaccessibility or damaging or hostile exposure conditions
- Interrogate entire field without the need to scan everywhere
- Devices may not be well characterised by analytical formulations
- With a set of measurements, now able to simulate through a variety of different materials

Disadvantages

- Measurements require expensive equipment and some experience
- Simulations can be computationally expensive
- Limited applications with regard to electronic steering etc

Ultrasound can be used to deliver acoustic, mechanical or thermal effects and the measurands may be based on this.

“All models are wrong, but some are useful.”

Furthermore, it is difficult to decouple the governing equations and the solution methods.

Choice of model may be influenced by computational resources available.

Introduction

Acoustic Equations

Acoustic Holography

Data Quality

Post-Acoustics Computation

Heat Equations

Dose Equations

Updating Equations

Measurements

Acoustics Measurements

Thermal & Dosimetric Measurements

Conclusions

Acoustic equations may contain three features, i.e. for a homogeneous KZK-type equation

$$\frac{\partial p}{\partial t} = \underbrace{\frac{c_0}{2} \int_{-\infty}^t \nabla^2 p \, d\tau}_{\text{Diffraction}} + \underbrace{\frac{2}{c_0^3} \mathcal{L} [p; \alpha_0, \eta]}_{\text{Attenuation}} + \underbrace{\frac{\beta}{2\rho c_0^3} \frac{\partial p^2}{\partial t}}_{\text{Nonlinearity}}$$

- **Diffraction**: the property of a wave to spread as it propagates
- **Attenuation**: the absorption of the wave by the medium
- **Nonlinearity**: the change in the waveform as it propagates

The equations can be propagated forward or backwards in space and time.

Which Governing Equation and Which Numerical Scheme?

An appropriate choice of governing equation and numerical scheme can be formulated based on consideration of three factors:

1. Duration: time or frequency domain?
2. Nonlinearity: linear or nonlinear wave propagation?
3. Homogeneity of source and domain: can dimension of system be reduced?

Broadly, each choice influences the next. Also the more complex, the more difficult to perform both simulations and measurements.

Additionally, the implementation of perfectly matched layers is dependent on the governing equation [1].

This determines whether it is appropriate to work in the **time** or the **frequency** domain.

- Short, pulsed waves should be handled in the time domain
- Longer pulsed waves comprising of many hundreds cycles can be handled in the frequency domain

Typically time for a time-domain solver to reach a steady state is dependent on boundary conditions and the presence of multiple reflections from scatterers: in many cases this can be thousands of cycles. Care may be needed to handle numerical dispersion in this situation when using finite-difference time domain methods.

This determines whether it is appropriate to compute **linear** or **nonlinear** wave propagation

IEC 62556 defines a local distortion parameter, σ , determining quasi-linear regimes, $\sigma < 0.5$

- If in the time domain, the number of time steps needs to adequately resolve the highest harmonic.
- If in the frequency domain, the number of harmonics computed may need to be determined before computing.

If a shock forms care is needed in measurements to ensure that the bandwidth of the measurement device can record the high frequency components.

Furthermore, information is lost at a shock front, so that back propagation through a shock can not recover pre-shock measurements.

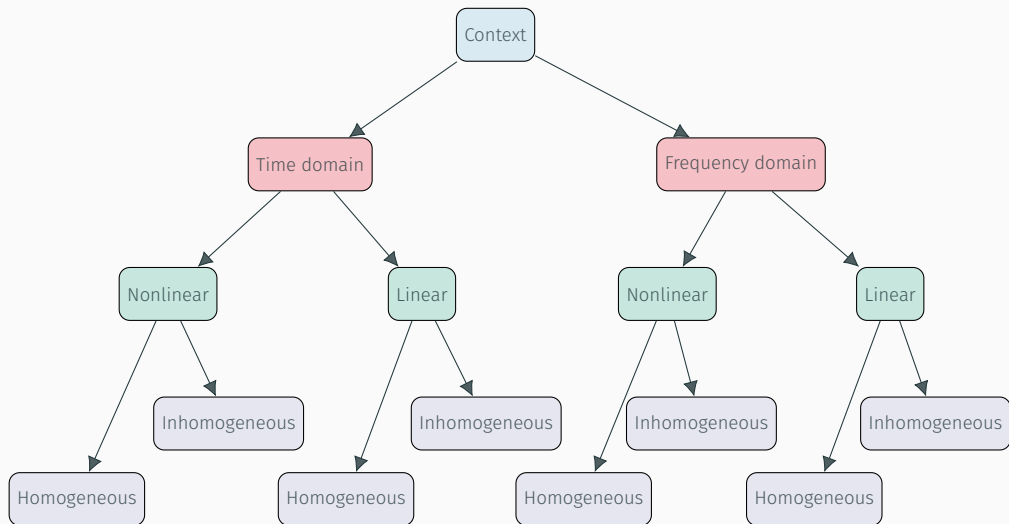
For **complex** media, exhibiting power-law attenuation, both duration and intensity influence the choice of attenuation operator:

- (time domain) distribution of relaxation processes [2]
- (pseudo-spectral spatial marching) fractional time-derivative [3]
- (pseudo-spectral time stepping) fractional Laplacian [4]

The duration and the intensity also determines the magnitude of the thermal field and any changes in material properties [5].

Paraxial approximation assumes essentially one-way propagation, but limits off-axis accuracy [6].

A Proposed Decision Tree



Introduction

Acoustic Equations

Acoustic Holography

Data Quality

Post-Acoustics Computation

Heat Equations

Dose Equations

Updating Equations

Measurements

Acoustics Measurements

Thermal & Dosimetric Measurements

Conclusions

- What is the required spacing between points, what is the size of the active element of the hydrophone and are spatial averaging corrections [7] required?
- Does the scan plane capture the complete acoustic field? Measuring pressure or velocity fields?
- If required, when is a steady state reached? Require a tone-burst which is of sufficient length to capture contributions from all of the transducer as well as avoiding ramp-up, but sufficiently short to not be effected by reflected signal, standing-waves, or electrical pick-up etc contaminating measurements.
- Is acquisition plane in linear regime?
- Ensure alignment of scan plane is known, so that measurement points can be related to computation points
- Ensure temperature of water is known (and stable)

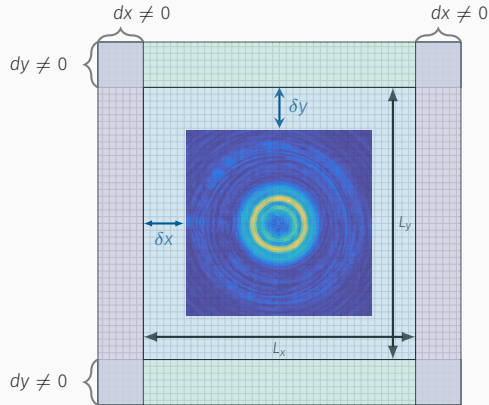


Figure 1: Schematic diagram of measurement (magnitude) data in computational domain and perfectly matched layers. Data can be padded and windowed.

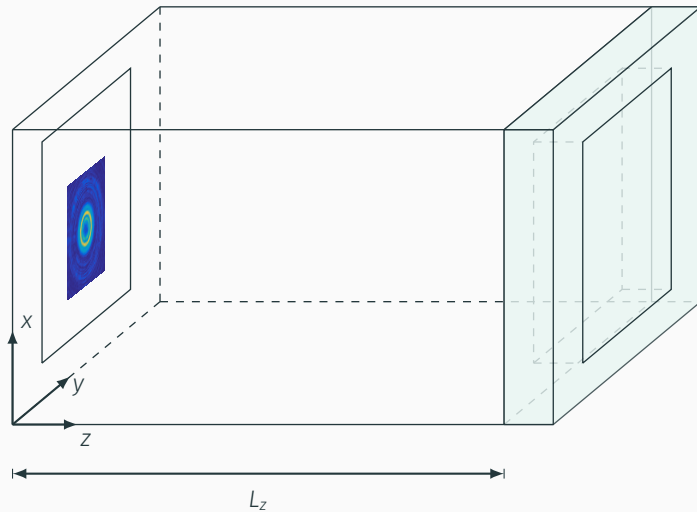


Figure: The axial distance, including a perfectly matched layer at the back to suppress spurious reflections.

Simple projections using Rayleigh integral methods can identify issues with alignment or coverage of scan plan etc.

The spectrum of the eigenvalues of the holography matrix suggests the data is **low-rank**.

Matrix completion techniques [8] can be used to:

- Identify outliers in the data
- Recover incomplete data

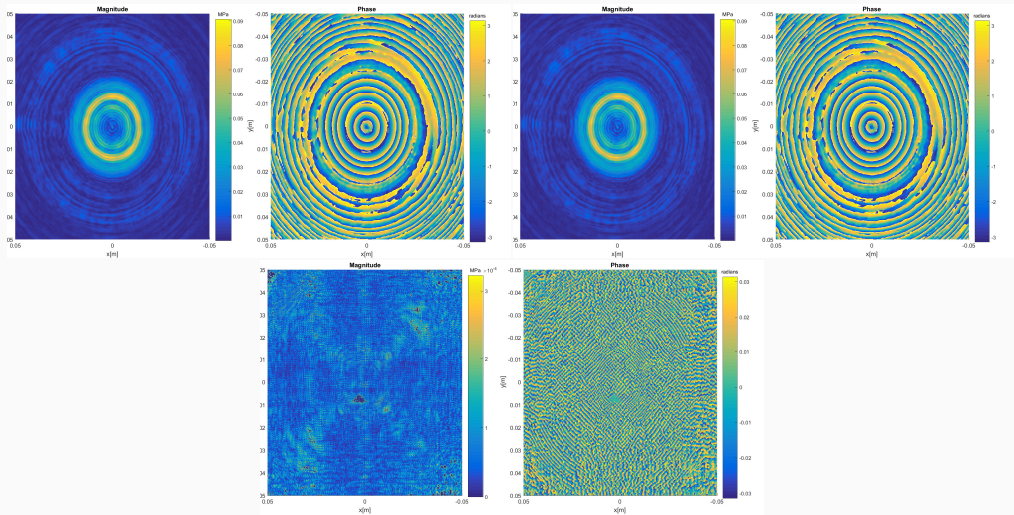


Figure 2: Measurement, reconstructed and errors from, which are from data with 70% of measurement data acquired.

Introduction

Acoustic Equations

Acoustic Holography

Data Quality

Post-Acoustics Computation

Heat Equations

Dose Equations

Updating Equations

Measurements

Acoustics Measurements

Thermal & Dosimetric Measurements

Conclusions

The standard bioheat equation [9]

$$\rho c_v \frac{\partial T}{\partial t} = \nabla (\kappa \cdot \nabla T) + \underbrace{\nu (T - T_\infty)}_{\text{bulk perfusion}} + q$$

Computational domain is typically smaller than acoustic field and spatial and temporal scales larger: impose Dirichlet conditions on down-sampled grid. Furthermore, heat equation spreads, with losses of fine-scale detail in comparison to acoustic field.

In the absence of shocks [10] and cavitation [11], the heat source, q , is proportional to $\nabla \cdot \langle \mathbf{v}p \rangle$ or, assuming particle velocity is in phase with the pressure, plane-wave approximation p^2 .

In the presence of shocks, an additional source term, independent of absorption, proportional to the **cube** of the shock height must be included.

Two formulations for the damage, Ω ,

- Arrhenius component models, based on chemical kinetic models. For example, the first-order rate equation

$$\textcircled{1}[E_a][r]^{k_d}[E_d] \quad \text{leads to} \quad \Omega = \int_0^t A e^{-E_a/(R\bar{T})} ds$$

- Cumulative equivalent minutes, typically threshold value of an isothermal dose value of 240 min at 43°

$$\Omega = \int_0^t R^{\bar{T}(x,t) - \bar{T}_{\text{ref}}} ds \quad \text{with} \quad \bar{T}_{\text{ref}} = 43^\circ \quad \text{and} \quad R = \begin{cases} 0.25 & \text{for } T < 43^\circ \\ 0.5 & \text{for } T \geq 43^\circ \end{cases}$$

Updating Equations

- Material properties will change with temperature, changing all fields. However, there is large additional computational cost through updating changes in material properties in the computational of deformation fields and, if in frequency domain, through the re-computation of the acoustic field.

What can change:

- Changes in material properties due to **deformation** this is dependent on both temperature and dose, experimental data exists for three component Arrhenius model [12]
 - Changes in material properties with **temperature** [5]
 - Changes in material **state**, i.e. due to boiling, which significantly alter some properties such as density [13]
-
- Furthermore, the rate at which material properties should be updated must be ascertained through a sensitivity study.

Introduction

Acoustic Equations

Acoustic Holography

Data Quality

Post-Acoustics Computation

Heat Equations

Dose Equations

Updating Equations

Measurements

Acoustics Measurements

Thermal & Dosimetric Measurements

Conclusions

There are a large range of potential uncertainties [14] in measurements

- Calibration uncertainty
- Directional response of hydrophone
- Bandwidth limitations for highly nonlinear waves
- Spatial averaging
- Complex-frequency response of hydrophone
- Alignment
- Changes in speed of sound due to temperature variations

Optical methods can also be used to rapidly interrogate acoustic fields in optically transparent materials [15]

Due to differing spatial and temporal scales, as well as the blurring effect of heat equation, validating temperature measurements is less precise, but with additional sources of uncertainties.

- Need to account for viscous heating artefacts in most thermocouples [16]

Comparing predicted dose fields requires accurate segmentation and registration of ablated volume and the computation of Dice or overlap scores.

Introduction

Acoustic Equations

Acoustic Holography

Data Quality

Post-Acoustics Computation

Heat Equations

Dose Equations

Updating Equations

Measurements

Acoustics Measurements

Thermal & Dosimetric Measurements

Conclusions

- Validation and verification requires combined consideration of governing equation and numerical scheme and is dependent on the context, i.e. is the desired outcome thermal or mechanical damage etc.
- There are uncertainties in both the measurement-based simulations and validation measurements: to date there is little rigorous uncertainty quantification of the full process [17]

- [1] Q.-H. Liu and J. Tao, “The perfectly matched layer for acoustic waves in absorptive media,” *J. Acoust. Soc. Am.*, vol. 102, pp. 2072–2082, 1997.
- [2] N. Jiménez, F. Camarena, J. Redondo, V. Sánchez-Morcillo, Y. Hou, and E. E. Konofagou, “Time-domain simulation of ultrasound propagation in a tissue-like medium based on the resolution of the nonlinear acoustic constitutive relations,” *Acta Acustica united with Acustica*, vol. 102, no. 5, pp. 876–892, 2016.
- [3] P. V. Yuldashev and V. A. Khokhlova, “Simulation of three-dimensional nonlinear fields of ultrasound therapeutic arrays,” *Acoust. Phys.*, vol. 57, no. 3, pp. 334–343, 2011.
- [4] B. E. Treeby and B. T. Cox, “Modeling power law absorption and dispersion for acoustic propagation using the fractional Laplacian,” *J. Acoust. Soc. Am.*, vol. 127, pp. 2741–2748, 2010.
- [5] I. M. Hallaj, R. O. Cleveland, and K. Hynynen, “Simulations of the thermo-acoustic lens effect during focused ultrasound surgery,” *J. Acoust. Soc. Am.*, vol. 109, pp. 2245–2253, 2001.
- [6] A. Bamberger, B. Engquist, L. Halpern, and P. Joly, “Parabolic wave equation approximations in heterogeneous media,” *SIAM J. Appl. Math.*, vol. 48, pp. 99–128, 1988.

- [7] D. Sinden, S. Rajagopal, N. C. Chaggares, G. Pang, and O. Ivanytskyy, "Reducing uncertainties for spatial averaging at high frequencies," in *2017 IEEE International Ultrasonics Symposium (IUS)*, pp. 1–4, IEEE, 2017.
- [8] A. E. Waters, A. C. Sankaranarayanan, and R. Baraniuk, "SpaRCS: Recovering low-rank and sparse matrices from compressive measurements," in *Advances in neural information processing systems*, pp. 1089–1097, 2011.
- [9] H. H. Pennes, "Analysis of tissue and arterial blood temperatures in the resting human forearm," *J. Appl Physiol.*, vol. 1, no. 2, pp. 93–122, 1948.
- [10] M. S. Canney, V. A. Khokhlova, O. V. Bessonova, M. R. Bailey, and L. A. Crum, "Shock-induced heating and millisecond boiling in gels and tissue due to high intensity focused ultrasound," *Ultrasound Med. Biol.*, vol. 36, no. 2, pp. 250–267, 2010.
- [11] C. C. Coussios, C. H. Farny, G. ter Haar, and R. A. Roy, "Role of acoustic cavitation in the delivery and monitoring of cancer treatment by high-intensity focused ultrasound (HIFU)," *Int. J. Hyperthermia*, vol. 23, no. 2, pp. 105–120, 2007.
- [12] J. Dueck, M. Marashdeh, and R. Breiter, "Experimental investigation and mathematical modeling of the thermal shrinkage of bovine pericardium," *J. Med. Biol. Eng.*, vol. 31, pp. 193–200, 2011.

- [13] J. P. Abraham and E. M. Sparrow, "A thermal-ablation bioheat model including liquid-to-vapor phase change, pressure- and necrosis-dependent perfusion, and moisture-dependent properties," *Int. J. Heat Mass Transf.*, vol. 50, no. 13-14, pp. 2537–2544, 2007.
- [14] E. Martin and B. E. Treeby, "Investigation of the repeatability and reproducibility of hydrophone measurements of medical ultrasound fields," *J. Acoust. Soc. Am.*, vol. 145, no. 3, pp. 1270–1282, 2019.
- [15] H. Luo, J. Kusunose, G. Pinton, C. F. Caskey, and W. A. Grissom, "Rapid quantitative imaging of high intensity ultrasonic pressure fields," *J. Acoust. Soc. Am.*, vol. 148, no. 2, pp. 660–677, 2020.
- [16] T. Tiennot, H. A. S. Kamimura, S. A. Lee, C. Aurup, and E. E. Konofagou, "Numerical modeling of ultrasound heating for the correction of viscous heating artifacts in soft tissue temperature measurements," *Appl. Phys. Lett.*, vol. 114, no. 20, p. 203702, 2019.
- [17] E. Neufeld, A. Kyriacou, W. Kainz, and N. Kuster, "Approach to validate simulation-based distribution predictions combining the gamma-method and uncertainty assessment: Application to focused ultrasound," *J. Verif. Valid. Uncert.*, vol. 1, no. 3, 2016.